

Effect of Ions Released and pH of Two Glass Ionomer Cements in Human Gingival Fibroblasts

Efecto de la liberación de iones y pH de dos cementos de ionómero de vidrio en fibroblastos gingivales humanos

Alejandro L. Vega-Jiménez DDS, MSc, PhD¹; Ana G. Rodríguez-Hernández DDS, MSc, PhD²;
María Cristina Piña-Barba PhD³; Javier Ambrosio-Hernández PhD⁴

1. Laboratory of Tissue Bioengineering. Faculty of Dentistry, Division of Postgraduate Studies and Dental Research. National Autonomous University of Mexico, Mexico.
2. CONACyT Research Fellow at Center of Nanoscience and Nanotechnology. National Autonomous University of Mexico, Ensenada, Baja California, Mexico.
3. Department of Ceramic Materials. Institute of Materials Research. National Autonomous University of Mexico, Mexico.
4. Department of Microbiology and Parasitology. Faculty of Medicine, National Autonomous University of Mexico, Mexico.

Correspondence to: Dr. Alejandro L. Vega-Jiménez - dr.vegalex@gmail.com

Received: 14-IX-2018

Accepted: 9-X-2018

Published Online First: 16-X-2018

DOI: <https://doi.org/10.15517/ijds.v0i0.34886>

ABSTRACT

Conventional glass ionomer cements are used as dental provisional restorative materials, which present several advantages such as adhesion to the tooth mineral phase among others. On the other hand, the knowledge about biological property of glass ionomers shows various approaches and results. In this work, it was studied the *in vitro* biological response of human gingival fibroblasts in contact with commercial cements of glass ionomer: Mirafil® and longlass® and with their extracts, according to ISO 10993. The extracts of the cements, in which the cells were cultured, were adjusted at different concentrations ranging 0.1% to 100%. The cellular metabolic activity of gingival fibroblasts was measured using the Alamar Blue® reagent. The results showed a significant effect on the cellular metabolic activity correlated with the concentration of liberated ions (Al^{3+} and Ca^{2+}) for both ionomers, as well as the pH variations of the culture media. This could mean that the cellular metabolic activity is substantially influenced by ions and pH of the cell culture.

KEYWORDS

Glass ionomer cement; Dental cement; pH; Ions; Cytotoxicity test; Cell culture; Cell viability.

RESUMEN

Los cementos de ionómero de vidrio convencionales se utilizan como materiales de restauración provisional para uso dental, los cuales presentan varias ventajas como la adhesión a la fase mineral de los dientes. Por otro lado, las propiedades biológicas de los ionómeros de vidrio muestran diversos enfoques y resultados. En éste trabajo se estudió la respuesta biológica *in vitro* de fibroblastos gingivales humanos en contacto con cementos comerciales de ionómero de vidrio: Mirafil® e longlass® y con sus respectivos extractos según la norma ISO 10993. Los extractos de los cementos en los que se cultivaron las células estaban en diferentes concentraciones: de 0.1% a 100%. La actividad metabólica celular se midió usando el reactivo Alamar Blue®. Los resultados mostraron un efecto significativo sobre la actividad metabólica celular correlacionada con la concentración de iones liberados (Al^{3+} y Ca^{2+}) para ambos ionómeros, así como las variaciones de pH de los medios de cultivo. Ello podría explicar la influencia por los iones y el pH del cultivo celular en la actividad metabólica celular.

PALABRAS CLAVE

Cemento de ionómero de vidrio; Cemento dental; pH; Iones; Ensayo de citotoxicidad; Viabilidad celular.

INTRODUCTION

Conventional glass ionomer cement (GIC) consist of an aqueous polyalkenoic acid (polyacrylic acid), which react with powder of calcium fluoro alumino silicate glass under acid-base reaction (1). GICs have several important properties such as: 1) fluoride release, which confers antibacterial effect and enhance hardness of mineral phase as dental enamel as well dentine (2); 2) thermal expansion coefficient and module of elasticity similar to the dentin (3) and 3) the physical and chemical adhesion of GIC on both enamel and dentin is physical and chemical (4). These properties have considered that this cement one of the most used materials in the dental practice. The cytotoxic effects of GIC in direct contact with fibroblasts have been documented in some cell culture studies (5-9). In this sense, released metal ions have been suggested as a cause of cytotoxicity, which are liberated from GIC in its initial setting phase. On the other hand, particles such as

alumina had been identified in cultivated cells on surface of set glass ionomers, where they had no visible detrimental effect (10,11). Furthermore, pH reduction during cements setting and maturing process has been suggested too as a cause of cyto and neurotoxicity, which might be related with the presence of acrylic acid in GICs (12). Is important to mention that studies on biocompatibility need to be carried out during evaluation of dental materials, since this is a major requirement, especially when they have been considered for implantation (12-14) and adapted for use in the implant abutment cement-retained crown (CRC) technique for the intimate contact with gingiva (15). Hence, the aim of this study was to evaluate the *in vitro* biological response of human gingival fibroblasts incubated with two conventional glass ionomer cements by Alamar Blue® reagent using two different tests; direct and extract contacts. Finally, the study was carried out in order to perform an analysis of the influence of both pH variations and ions released in the viability and cytotoxicity.

MATERIALS AND METHODS

GLASS IONOMER SAMPLES

Two commercial GICs were used: longlass® (Viarden SA de CV, Mexico) and Mirafill® (Faprodmir, Germany). Samples were prepared according to powder/liquid ratio mixture indicated by each manufacturer; then samples were placed under temperature ($37\pm 1^\circ\text{C}$) and humidity (90%) controlled for one hour according to ANSI/ADA Standard No. 96. The samples were immersed in deionized water and stored in an oven at 37°C for 24 hours. Previous cell culture experiments, all samples were sterilized under UV radiation inside of a laminar flow cabinet for 40 min. The surfaces of materials were observed by Scanning Electron Microscopy (SEM) JEOL 5600 LV with secondary electrons at 20 keV.

DETECTION OF RELEASED IONS FROM GICS AND PH MEASUREMENTS IN DMEM

The elements released in DMEM from GIC samples (As^{5+} , Pb^{2+} , Al^{3+} , Ca^{2+} , Na^+ , K^+) were measured by Atomic Absorption Spectroscopy (AAS 3100 Perkin Elmer®). Previously, 4mL of each extract were digested in Teflon® reactors with 1mL of HNO_3 and 1.25mL of HCl at 90°C for 8 h. Therefore, 0.25 mL of LaO_3 was added and solutions were gauged until final volume of 25mL. Whereas, pH variations in culture media were monitored at 12, 24, 36, 48 and 72 hours through the use of a pHmeter (pH HANNA® 213).

CELL CULTURE ASSAYS

Previous to material-cell experiments, human gingival fibroblasts [15] were grown and maintained in Dulbecco's Modified Eagle's Medium (DMEM GIBCO®), supplemented with 10% Fetal Bovine Serum (FBS GIBCO®), 8mM L-glutamine (GIBCO®) and penicillin (50,000 units/mL)/streptomycin (50 mg/mL) (GIBCO®) at 37°C and 5% CO_2 . For

each sort of experiment 40,000 fibroblasts per well were seeded in 24 multiwell culture plates (Nunc®) and incubated during 4 hours until cells spreading. Cell-materials experiments were performed with extracts of GICs in culture media as well as cell material direct as is indicated below. In both experiments, cell viability was assessed by monitoring their metabolic activity using Alamar Blue® (ABr) (Invitrogen®), measurements were collected at 570 nm wavelength in a spectrophotometer Benchmark Plus (BIO-RAD®) at 600 nm wavelength of reference).

CELL-EXTRACT MATERIAL ASSAY

Extracts were obtained from GIC Mirafill® as well as longlass® after 72 hours of incubation at 37°C in supplemented DMEM. 4 discs of 15 mm diameter and 4.5mm thickness were incubated in 11mL of culture media, according to ratio 3mm²/mL established into standard ISO 10993-5 guidelines. Under these conditions, we defined the media recovered as initial extract (100%) that contained the total amount of released ions. Finally different dilutions were prepared from initial extract: 50%, 10%, 1% and 0.1%. Chlorine (Cl) was used as positive control of cytotoxicity, whereas supplemented DMEM was the negative control. Cells were incubated with GICs extract and controls for 12 hours at 37°C and 5% CO_2 in 24 multiwell plate. At the same time, different amount of cells (since 300 until 50,000) were seeded in order to obtain a standard curve (relation between number of cells and absorbance). Then 10% of ABr was added to all cell cultures, according to O'Brien procedure (13), and plates were again incubated for 12 hours. 100 μL from each well were placed into 96 multiwell plate and absorbance was measured. At the end of the incubation, fibroblast morphology was observed using a light conventional microscopy with an inverted microscope NIKON® TS100. Images were taken with a digital camera (DS-Fi1-U2, NIKON®) and processed with software NIS Elements F® V 3.0.

DIRECT CONTACT CELL-MATERIAL ASSAY

For this experiment, GIC and controls disc of 4 mm diameter and 6 mm thickness (Alumina as negative control and PVC as positive control of cytotoxicity) were placed directly in contact with cells into 24 multiwell culture plate, according to standard ISO 10993-5 guidelines. 10% of ABr was added to each well and cells were incubated during 72 hours at 37°C and 5% CO₂. Measurements of absorbance were carried out at 12,24,36,48 and 72 hours of incubation by removing 100 µL of supernatant and placing them into a 96 multiwell plate.

STATISTICAL ANALYSIS

Statistical analysis was performed by analysis of variance (ANOVA) and Tukey was applied as multiple range test post hoc using software Origin 6.1, with a significance level of $p=0.05$. The analyses were performed with the results of direct cell-material contact and extract of three independent experiments.

RESULTS

SEM IMAGES OF GLASS IONOMER SAMPLES

SEM micrographs of GICs before cell culture assay are shown in Fig.1. Both surfaces presented cracks, which were more in quantity and extension on Mirafill® (Fig.1-A) compared to longlass® (Fig.1-C). To the contrary, higher porosity and embedded particles were observed on longlass® (Fig.1-B) than Mirafill® surface (Fig.1-D).

RELEASED IONS FROM GICS AND PH MEASUREMENTS IN DMEM

Ions liberated to culture media from both GICs, were presented in table 1, where just Al³⁺ and Ca²⁺ were detected in DMEM after 72 h of incubation with both materials, according to standard ISO 10993 guidelines. Presence of Al³⁺ was just

found in longlass®; whereas Ca²⁺ was detected in both GICs, presenting a higher concentration in Mirafill®. On the other hand, pH variations due to presence of GICs in culture media are shown in table 2. In the beginning, the culture media had a neutral pH, which decrease slightly from 7.40 ± 0.02 until 7.2 ± 0.1 for Mirafill® CIG after 36 hours of immersion in DMEM; while longlass® presented a more sudden decrease (from 7.40 ± 0.02 to 6.7 ± 0.1) for the same immersion time. Subsequently in both cases, pH remains constant in the time.

CELL CULTURE ASSAYS

EFFECT OF RELEASED IONS ON GINGIVAL FIBROBLASTS

The results of cell cytotoxicity and their relation with both GIC extract concentration are presented in Table 1 and plotted in Figure 2. As can see in this figure, there is an inversely proportional response between the number of viable cells and the extract concentration. The negative control presented a maximum number of viable cells (represented as black bar) which drop abruptly after just an extract dilution of 0.1%. Even this decrement was observed for both materials, longlass® presented a higher cytotoxic effect compared to Mirafill® with a cell viability of 39% (20581 ± 68 cells) versus 68% (36206 ± 94 cells) respectively.

Following dilutions presented a continuous decrease on number of viable cells, where longlass® maintained a higher cytotoxicity compared to Mirafill®. Finally, positive cytotoxic control presented a minimum number of viable cells (189 ± 56). Statistical analysis by factorial ANOVA followed by Tukey test; showed significant differences between Mirafill® and longlass®. Furthermore, both GICs at all concentrations, presented significant differences ($p<0.05$) with the negative control group.

At the same time, variation of ions concentration (Ca²⁺ and Al³⁺) and pH for different

GIC extract dilutions are shown in figure 3. These dates were obtained from initial and final value of each measurement and applying the rule of mixtures, the intermediate points were obtained. In the case of Mirafill® just Ca²⁺ was detected, whilst longlass® liberated both Ca²⁺ and Al³⁺ (Fig.3-A). Whereas pH variations of culture medium presented a lower pH values of longlass® compared to Mirafill® (Fig.3-B).

DIRECT CONTACT CELL-MATERIAL ASSAY

Results of cell-material interaction with both GICs and controls are shown in Figure 4. In the image is possible to observe the well defined cell culture trend for each sort of sample. During the cell culture time, the cells were growing in a similar tendency, reaching a maximum between 30 to 50 h.

The statistical analysis, showed that when cells were cultured with alumina was practically identical to Tissue-culture treated polystyrene

(TPS) measurements during all incubation time and no significant differences were observed ($p > 0.05$). While GICs results are presented almost the same tendency and measurement without significant differences ($p > 0.05$) between them since 24h until 72 h, but at 12 h of incubation significant difference ($p < 0.05$) was observed, because cells in contact to Mirafill® presented a few decrement in its absorbance. Furthermore, both GICs presented significant differences vs alumina at 12, 24 and 36 h of incubation. Whereas, PVC results showed the lowest absorbance results compared to others ($p < 0.05$)

In order to associate the effect of pH variation in cell viability during incubation, data were plotted versus absorbance for both glass ionomers (Figure 5). Results are showed that cell viability in both cases appear have not be affected by pH variations, because of cells viability was not compromised in presence neither longlass® as is shown in Fig. 5-A (even pH decrease until 6.5), nor Mirafill® (Fig. 5-B).

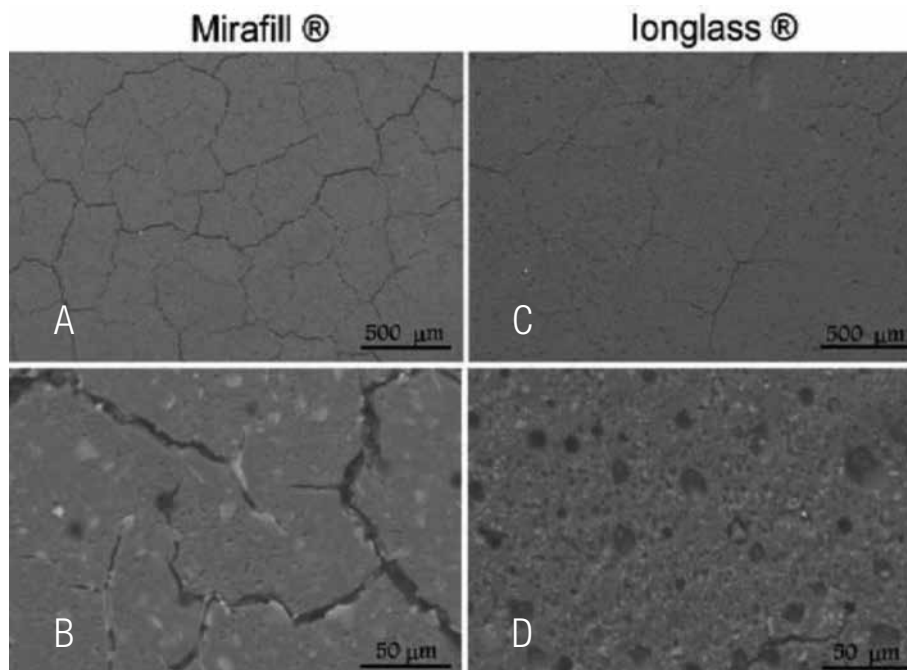


Figure 1. SEM images from Mirafill® (A and B) and longlass® (C and D). The presence of cracks was more evident in Mirafill®, whereas longlass® presented a more porous surface.

Table 1. The absorbance, the cell count and the Ca²⁺ and Al³⁺ concentrations measured in the culture media for the different concentrations of the extract are shown.

Extrat concentration (%)	Absorbance (570 nm)	NO.Cells	Ca ²⁺ concentration (µg/mL)	Al ³⁺ concentration (µg/mL)
longlass®				
100	0.264±0.04	4726±98	67	8
50	0.275±0.02	7560±67	61	4
10	0.295±0.009	10881±51	56.2	8
1	0.318±0.002	16803±47	55.1	ND
0.1	0.329±0.02	20581±68	ND	ND
Mirafill®				
100	0.271±0.005	6945±49	86	ND
50	0.301±0.001	12243±45	70.5	ND
10	0.324±0.003	18673±83	58.1	ND
1	0.353±0.04	31913±109	55.3	ND
0.1	0.359±0.04	36206±94	ND	ND
Controls				
Positive	0.077±0.01	189±56	ND	ND
Negative	0.380±0.004	53312±48	55	ND

Table 2. Variation of pH during GICs incubation in DMEM for different times. Data represented are the mean and standard deviation of three isolated experiments.

		Time (h)				
		12	24	36	48	72
pH	Mirafill®	7.36±0.02	7.33±0.02	7.2±0.01	7.18±0	7.18±0
	longlass®	7.26±0.02	7.03±0.02	6.8±0.2	6.7±01	6.7±0.1

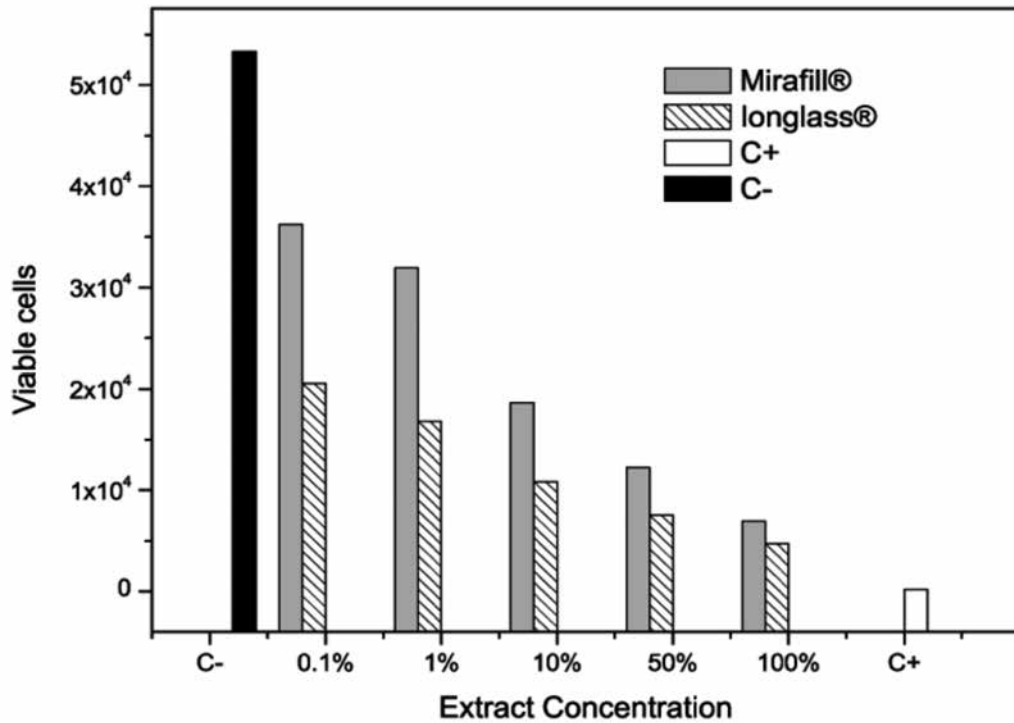


Figure 2. Data of extract concentration and the amount of survivor cells (Data plotted represent the media and the standard deviation of 3 independent assays. For the scale the error bar is not evident), compared to negative (white) and positive (black) control of cytotoxicity.

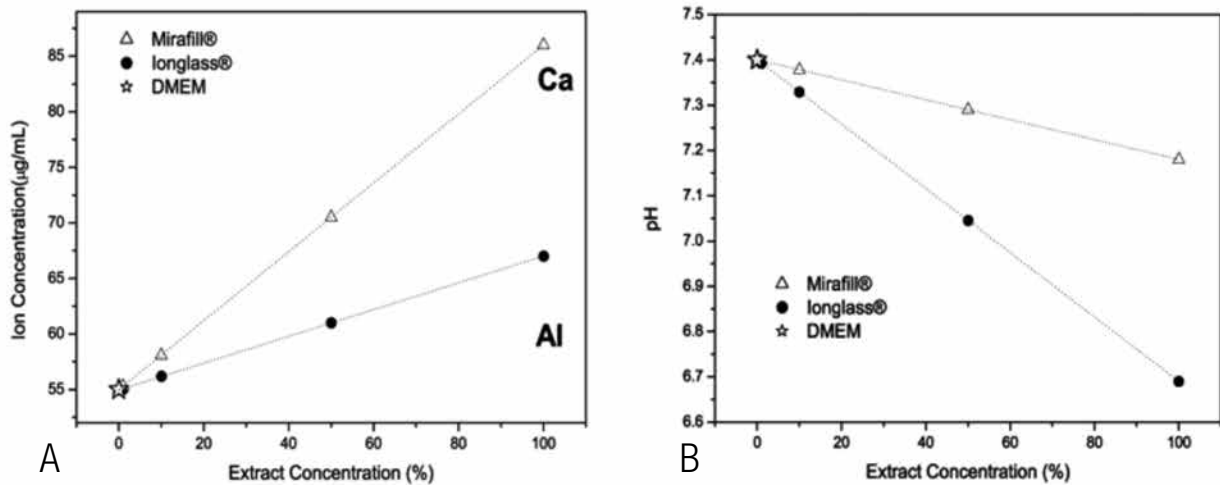


Figure 3. Extract concentration vs the amount of Ca²⁺ and Al³⁺ (A) and vs pH (B).

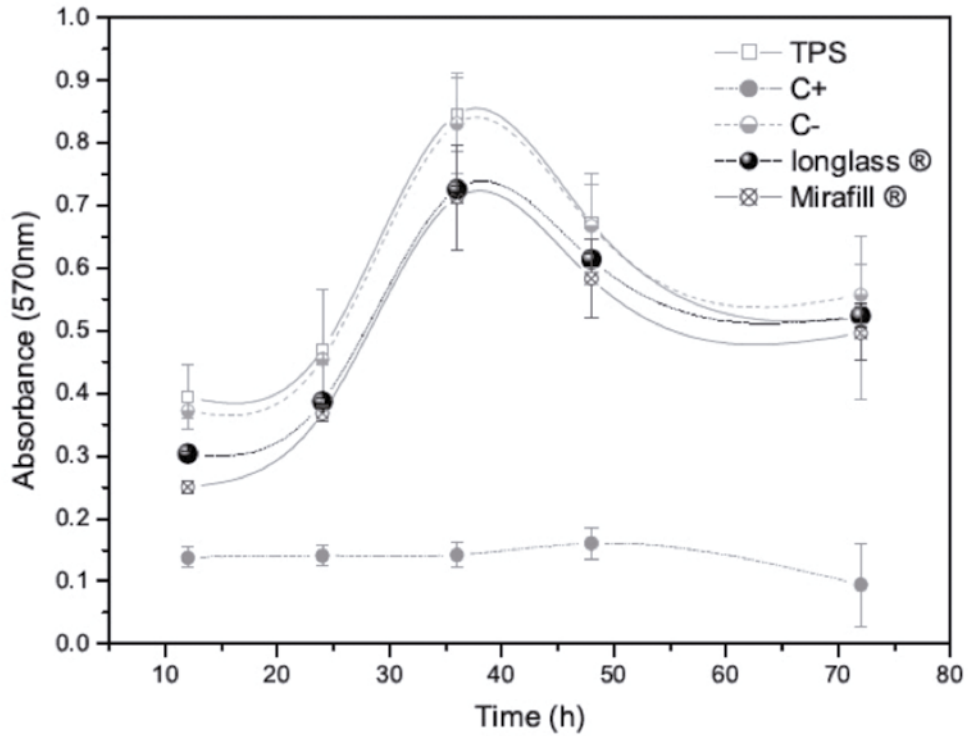


Figure 4. Through the absorbance of the cell culture, by putting the cells in direct contact with the culture plate (TPS), the positive (PVS) and negative (Al2O3) and the GICs considered, we can measure the cell viability, we can measure the cell viability, which is approximately 88%.

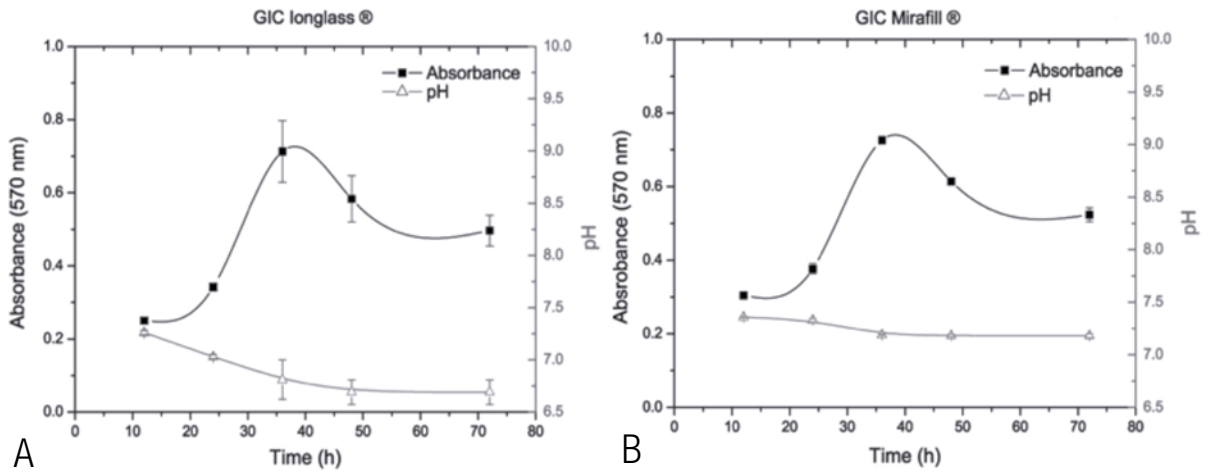


Figure 5. The pH of the cell culture medium, in the ionomers presence remains practically constant over time, as can be seen in graphs A and B. The change is a little higher in longlass case.

DISCUSSION

In this study, the evaluation of cytotoxicity and viability of human gingival fibroblasts in presence of two conventional glass ionomers, have evidenced two important facts: first, the effect of ion released concentration on cell cytotoxicity; and second, the adaptability of cells to environment, due to fibroblasts viability trend in presence of both GICs, besides variations of pH in culture media.

With respect to GIC cytotoxicity is important to point out that leachables from glasses ionomers are released during early contact with environment, fact well known due to glass ionomers present high solubility during initial 24h (16). This effect can be observed as well pH variation of culture medium as the variations in cell viability. Some authors have shown that dental glass ionomers can release some substances, compounds and elements such as non polymerized monomers, polyacid, fluoride (17), Al^{3+} (12), Ca^{2+} , silica, phosphates (18,19), Pb and As (17) that are considered to produce an effect on cell viability (20). However, lead and arsenic were not found in this work.

Nevertheless, variations correlated to Ca^{2+} and Al^{3+} concentrations in DMEM seem to be the responsible of cell viability. Fact corroborated in results of both ionomers, which have shown a well defined trend correlated to extract concentration, because of the amount of viable cells decrease when extract concentration increase. Into literature there are some reports about importance of Ca^{2+} in cellular signalling, cell interactions and cell cycle (21). As we could observe, the variation of this ion had a critical effect in cell viability, due to Ca^{2+} concentration at 50% for both ionomers showed a significant difference between cells (higher Ca^{2+} concentration = more cells); however at 100% of concentration the difference previously observed, almost have disappeared. These results show clearly the effect of Ca^{2+} in cell viability which are

able to sense these small variations, but did not explain the cytotoxic observed. That effect may be more related to Al^{3+} (22) and pH concentration.

In the first case the presence of that ion was just detected in longlass® which presented the fewer amounts of cells. With respect to pH and according to rule of mixtures, (Fig.3-B) the pH variation is more related to cell viability, because the lower pH presented the fewer amount of cells that correspond to longlass® results.

Furthermore, with respect to cells adaptability was well evidenced that initial hours of the cell culture, seems to be crucial in the viability of fibroblasts, because of at this time there were significant differences in the number of viable cells. Subsequently, there appears to be an adaptation of the cells in the presence of the material, as they follow a similar behavior in both the negative control (alumina) and growing under normal *in vitro* conditions. Although, pH has been considered a critical factor of cell viability and cytotoxicity (23), our results showed that pH by itself did not have a determinant effect in cell *in vitro* growth. This behavior may be explained by a cell modification and adaptation environment process, that allow them continue with their cycle, because of as we observed the numbers of cells are almost equaled, completely independent of pH variations.

The results obtained allowed to identify that the cytotoxic effect caused for each component and, the cellular adaptability to surrounding environment changes. In the first case, was observed how the concentration of Al^{3+} and pH affect survivor cells whereas in the second case, the cell viability results showed the adaptability of cells to variations in culture conditions, due to cells in presence of both ionomers presented the same amount of cells between them, and both are following a similar behavior in contact with Al_2O_3 as well as TPS.

Is important to point of that, even the clinical situation is different due to concentration of elements released, they are diluted in the saliva and the mucosa surface that acts as barrier; *in vitro* studies provide a significant amount of information that permit to elucidate the response of cell into a toxic environment.

CONCLUSIONS

According with the results, we can conclude that concentration of products released in the culture medium from the GICs presented a well defined effect in the cellular cytotoxicity. This effect could be originated by the fibroblast metabolic activity that substantially affected by ions and pH of cell culture, and it has been higher in cells incubated with longlass®. This essay is useful for evaluation of threshold limit of toxic products. And with respect to viability results, data showed the adaptability of cells to their environment variations, that can be consider as better assay to evaluate cell cytotoxicity of implantable potentially materials.

FUNDING

This work was financially supported by Faculty of Dentistry, Institute of Materials Research, Faculty of Medicine (UNAM) and DGAPA-UNAM projects: IT104011, IN201510, IN224316 and IX200610.

CONFLICT OF INTERESTS

The authors declare no conflicts of interest.

COMPLIANCES WITH ETHICS GUIDELINES

This article does not contain any studies with human or animal subjects performed by any of the authors.

ACKNOWLEDGEMENTS

Cells were donated by Dr. Juan Antonio Arreguín-Cano from the Faculty of Dentistry, UNAM. Technical support was provided by Dra. Miriam Marin-Miranda of the Department of Dental Materials at the Dental School from the Faculty of Postgraduate and Studies Zaragoza UNAM, MSc Margarita Linares Zapién and Dr. Federico Barceló-Santana. QFB Maria Guadalupe Espejel performed ion analysis in the Laboratory of Atomic Absorption Spectroscopy at the Postgraduate of the Faculty of Chemistry UNAM. Vega-Jiménez wants to thank to CONACYT (Scholarship No. 330328) and Rodríguez-Hernández wants to thank DGAPA-UNAM for the awarding of the postdoctoral scholarship program.

DISCLAIMER

The content of the manuscript is solely responsibility of the authors and does not necessarily represents the official views of the National Autonomous University of Mexico.

REFERENCES

1. Monmaurapoj N., Soodsawang W., Tanodekae W., Channasanoo N. Effect of Glass Preparation on Mechanical Properties of Glass Ionomer Cements. *J of Metals, Materials and Minerals* 2010; 20: 197-9.
2. Gao W., Smales R. J. Fluoride release/uptake of conventional and resin-modified glass ionomers, and compomers. *J Dent* 2001; 29: 30-6.
3. Bullard R. H., Leinfelder K. F., Russell C. M. Effect of coefficient of thermal expansion on microleakage. *J Am Dent Assoc* 1998; 116: 871-4.
4. Erickson R. L., Glasspoole E. A. Bonding to tooth structure: a comparison of glass

- ionomer and composite-resin systems. *J Esthet Dent* 1994; 6: 22-44.
5. Leyhausen, G., Abtahi, M., Karbakhsh, M., Sapotnick, A., & Geurtsen, W. Biocompatibility of various light-curing and one conventional glass-ionomer cement. *Biomaterials*, 1998; 19 (6), 559-564.
 6. Schmid-Schwap M., Franz A., Cytotoxicity of four categories of dental cements. *Dent Mater* 2009; 25: 360-8.
 7. Koulaouzidou, E. A., Papazisis, K. T., Economides, N. A., Beltes, P., & Kortsaris, A. H. (2005). Antiproliferative effect of mineral trioxide aggregate, zinc oxide-eugenol cement, and glass-ionomer cement against three fibroblastic cell lines. *Journal of Endodontics*, 2005; 31 (1), 44-46.
 8. Schedle A., Franz A., Rausch-Fan X. H., Spittler A., Lucas T., Samorapoompichit P., Sperr W., Boltz-Nitulescu G. Cytotoxic effects of dental composites, adhesive substances, compomers and cements. *Dent Mater* 1998; 14: 429-40.
 9. Sasanaluckit, P. A. K. R., Albustany, K. R., Doherty, P. J., & Williams, D. F. (1993). Biocompatibility of glass ionomer cements. *Biomaterials*, 14 (12), 906-916.
 10. Sidhu S., Schmalz G. The biocompatibility of glass ionómero cements materials. Status report. *Am J Dentistry* 2001; 14: 387-96.
 11. Hatton P., Hurrell-Gillingham K., Brook I. Biocompatibility of glass-ionomer bone cements. *J Dent* 2006; 34: 598-601.
 12. Brook I., Hatton P. Glass-ionomers: bioactive implant materials. *Biomaterials* 1998; 19: 565-71.
 13. Giacomelli E., Gonçalves E., Mitsuo H., Belle R., Mayumi L. Development of glass ionomer cement modified with seashell powder as a scaffold material for bone formation. *Rev Odonto Cienc* 2011; 26: 40-4.
 14. Giannoudis, P. V., Dinopoulos, H., & Tsiridis, E. (2005). Bone substitutes: an update. *Injury*, 36 (3), S20-S27.
 15. Sheets, J. L., Wilcox, C., & Wilwerding, T. (2008). Cement Selection for Cement-Retained Crown Technique with Dental Implants. *Journal of Prosthodontics*, 17 (2), 92-96.
 16. Shen C. Dental Cements. In: Anusavice KJ, editor. *Phillips' Science of Dental Materials*. 11st ed. Missouri USA: Saunders Elsevier; 2007. Pp. 474.
 17. Øilo G. Biodegradation of dental composite/glass ionomer cements. *Adv Dent Res* 1992; 6: 50-4.
 18. Yli-Urpo, H., Vallittu, P. K., Närhi, T. O., Forsback, A. P., & Väkiparta, M. Release of silica, calcium, phosphorus, and fluoride from glass ionomer cement containing bioactive glass. *Journal of biomaterials applications*, 2004; 19: 5-20.
 19. Oliva A., Della Ragione F., Salerno A., Riccio V., Tartaro G., Cozzolino A., D'Amato S., Pontoni G., Zappia V. Biocompatibility studies on glass ionomer cements by primary cultures of human osteoblasts. *Biomaterials* 1996; 17: 1351-6.
 20. Sjögren S., Sjögren G., Effects of glass ionomers and dental resin composites on viability of b-cells and insulin release in isolated islets of Langerhans. *Biomaterials* 2003; 24: 37416.
 21. Machaca K., Ca²⁺ signaling, genes and cell cycle. *Cell calcium* 2010; 48: 243-50.
 22. Lönnroth E., Einar J. Cytotoxicity of dental glass ionomers evaluated using dimethylthiazol diphenyltetrazolium and neutral red tests. *Acta Odontol Scand* 2001; 59: 34-9.
 23. Nicholson J., Czarnecka B., Review Paper: Role of aluminum in Glass-ionomer dental cements and its biological effects *J. Biomaterials Applicate*. 2009; 24: 293-308.



Attribution (BY-NC) - (BY) You must give appropriate credit, provide a link to the license, and indicate if changes were made. You may do so in any reasonable manner, but not in any way that suggest the licensor endorses you or your use. (NC) You may not use the material for commercial purposes.